

IONIZÁLÓ SUGÁRZÁS HATÁSA AZ ÉLŐ KÖRNYEZETRE MEASUREMENT TECHNIQUES

Szegedi Domonkos

BME Institute of Nuclear Techniques

National Institute of Oncology

- **Multiple Exposures: Chronicles of the Radiation Age**
- **487/2015. (XII. 30.) Korm. Rendelet az ionizáló sugárzás elleni védelemről és a kapcsolódó engedélyezési, jelentési és ellenőrzési rendszerről**
- **Köteles György: Sugáregészségtan**
- **Deme Sándor, Fehér István: Sugárvédelem**

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Dozimetry and measurement techniques - definitions

Dose concept

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- „dose” – quantity, portion (originally in medication)
- For quantitisation of ionising radiation
- Expressible in terms of basic quantities
- Beginning
 - Erythema dose – threshold dose of a deterministic effect
 - First dose limit among radiologists: 1/100 of the erythema dose per month (Mutscheller, 1924)

Absorbed dose

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- **Absorbed dose:** the ratio of the radiation energy absorbed by a given volume element to the mass of that volume element

$$D = \frac{\Delta\bar{\varepsilon}}{\Delta m}$$

- The unit of measurement is the **gray** (pronounced *grey*), symbol **Gy**,

$$1\text{Gy} = 1 \frac{\text{J}}{\text{kg}}$$

- In a differential approach, it can be used as a point quantity.

Dose, dose rate

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- To heat 1 kg of water by 1 °C, 4200 Gy is required
4 Gy is a semi-lethal dose for the human body
- **Dose rate (dose intensity)**

absorbed dose per unit time $\dot{D} = \frac{dD}{dt}$

$$\text{unit: } \frac{\text{Gy}}{\text{s}} = \frac{\text{J}}{\text{kg}} / \text{s}$$

Quantity	Radiation protection	Radiation therapy
Dose	<i>mGy, μGy</i>	<i>Gy, cGy</i>
Dose rate	<i>mGy/h, μGy/h</i>	<i>Gy/min, cGy/min</i>

Biological dose concept

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- The biological destructive effect of a given ionizing radiation shows variability depending, among other factors, on the type of radiation and the type of irradiated living tissue.
- **RBE – Relative Biological Effectiveness:**
the biological destructive effect of a given radiation type/quality, compared to 250 kV peak X-rays, for the same absorbed dose.

Equivalent dose

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Equivalent dose (H): takes into account the biological effectiveness of the given type of radiation (e.g. α , β , γ)

$$H_T = \sum_r w_r D_{T,r}$$

- Where $D_{T,r}$ is the absorbed dose in tissue **T** from radiation of type **r**, and w_r is the radiation weighting factor. Its unit is the **sievert**, 1 Sv = 1 J/kg

Equivalent dose

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Type of radiation	Weighting factor
Foton	1
Elektron, muon	1
Neutron <10keV	5
10keV-100keV	10
100keV-2MeV	20
2MeV-20MeV	10
20MeV<	5
Proton	5
Alfa particles	20

Effective dose

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- **Effective dose (E):** takes into account the specific radiosensitivity of a given organ or tissue

$$E = \sum_T w_T H_T$$

- Where H_T is the equivalent dose in tissue T, and w_T is the tissue weighting factor characterizing the radiosensitivity of that tissue. Its unit is the **sievert**, $1 \text{ Sv} = 1 \text{ J/kg}$

Effective dose

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Tissue	Tissue weighing factors	
	ICRP 60	ICRP 103
Gonade	0,2	0,08
Marrow	0,12	0,12
Lung	0,12	0,12
Breast	0,05	0,12
Thyroid	0,05	0,05
Bone surface	0,01	0,01
Colon	0,12	0,12
Stomach	0,12	0,12
Bladder	0,05	0,05
Liver	0,05	0,05
Skin	0,01	0,01
Esophagus	0,05	0,05
Other organs, tissues	0,05	0,12

Committed dose

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- **In case of incorporation, from the time of intake:**

Dose can be expressed in integral form

- **Time dependence of dose rate:**
 - **Biological half-life** – relates to the elimination from the body
 - **Physical half-life** – decrease in activity due to radioactive decay

$$H_T(\tau) = \int_{t_0}^{t_0 + \tau} \dot{H}_T(t) dt$$

Operative quantities

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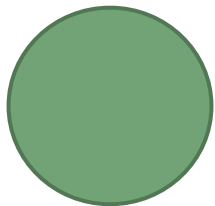
- Ambient dose equivalent
- Personal dose equivalent
- Directional dose equivalent to the lens and to the unit surface of the skin

ICRU phantom

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- 76,2% oxygen
- 11,1% carbon
- 10,1% nitrogen
- 2,6% hydrogen

1g/cm³ density, tissue-equivalent
plastic phantom



300 mm diameter
sphere phantom



(300x300x150) mm³
phantom

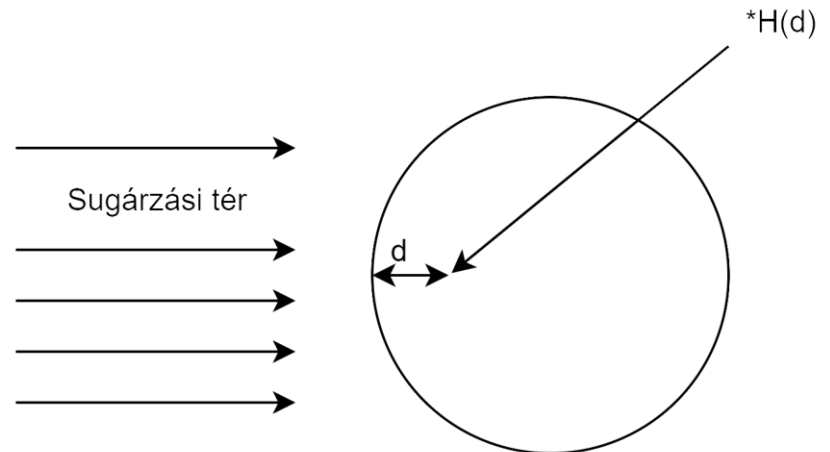
Ambient dose equivalent

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That dose equivalent at a given point in the radiation field which, **at a depth d in the ICRU sphere**, would be produced by the expanded and aligned radiation field corresponding to the dose equivalent, measured along the radius of the sphere opposite to the direction of the aligned beam.

High LET radiation: $d = 0,07 \text{ mm}$

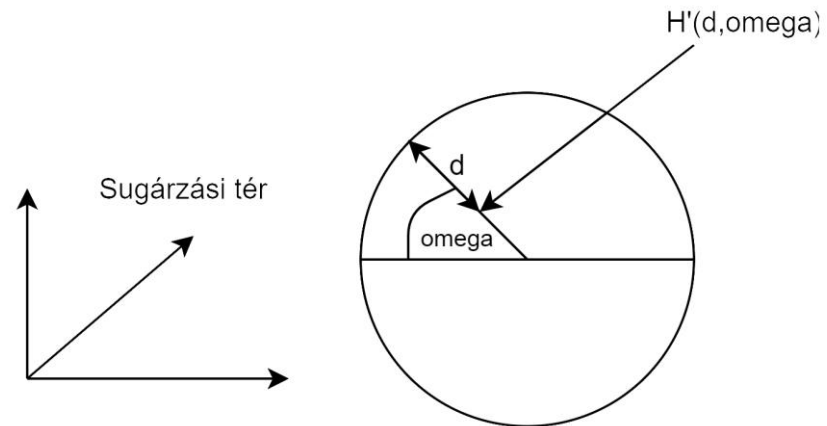
Low LET radiation: $d = 10 \text{ mm}$



Directional dose equivalent

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That dose equivalent at a given point (P) in the radiation field which, at a depth d in the ICRU sphere, would be produced by the expanded radiation field corresponding to the dose equivalent, measured along the radius of the sphere in the specified direction Ω .

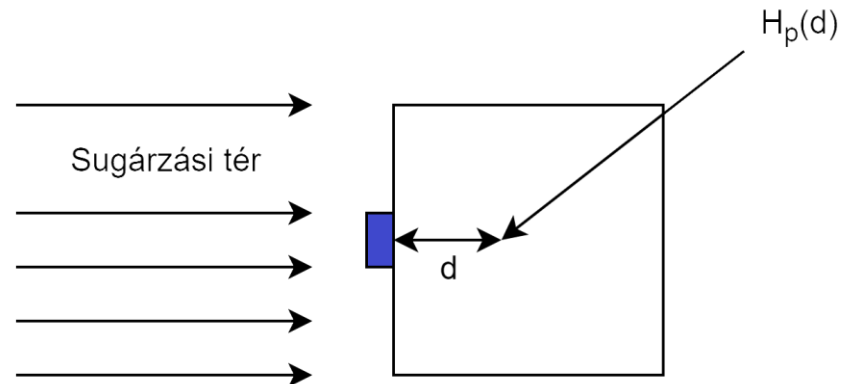


Personal dose equivalent

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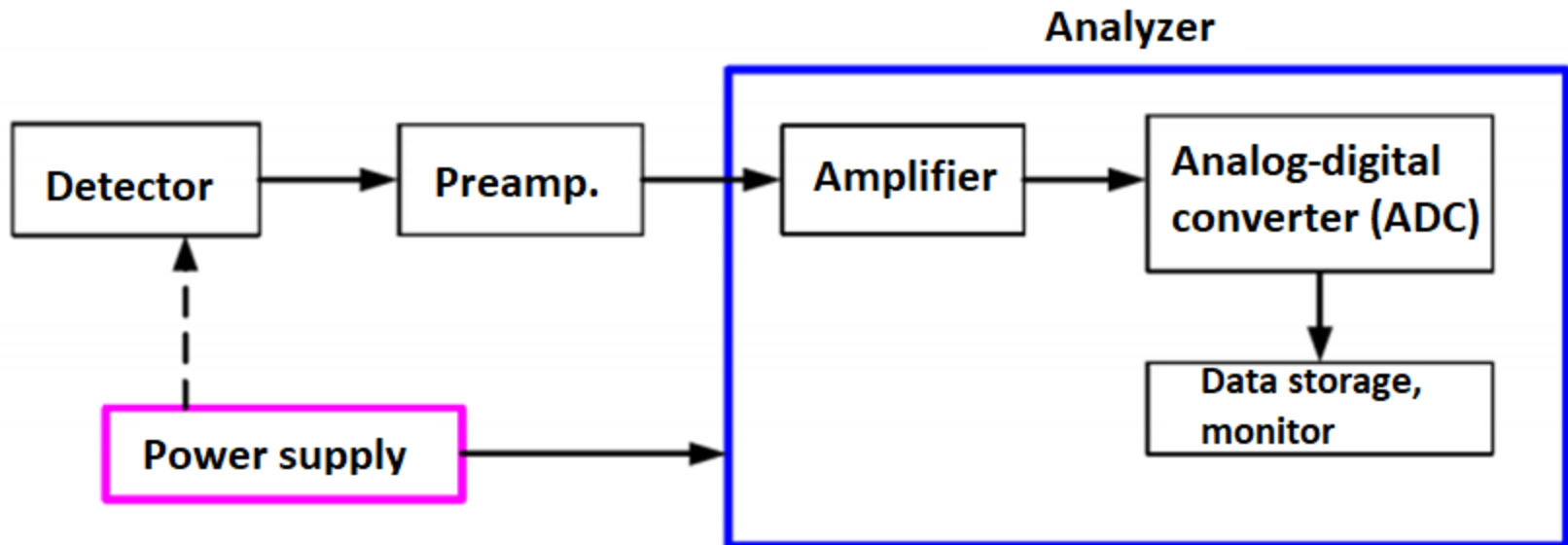
The dose equivalent in soft tissue located at a depth d below a specified point on the body surface.

The quantity used as the basis for workplace monitoring to estimate personal doses.



Detector systems

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Parts of the measurement system

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- **Detector**
- **Analog signal processing** (e.g., preamplification)
- **ADC (Analog-to-Digital Converter)**
- **Digital signal processing** (e.g., amplification)
- **Counting and data storage**
- **Optional: data processing with a multi-channel analyzer**

The type of detector determines the required electronics (e.g., photomultiplier), detection capabilities (e.g., qualitative analysis, dose measurement), and measurement conditions (e.g., cooling, additional shielding, underwater measurement).

Detection of ionizing radiation

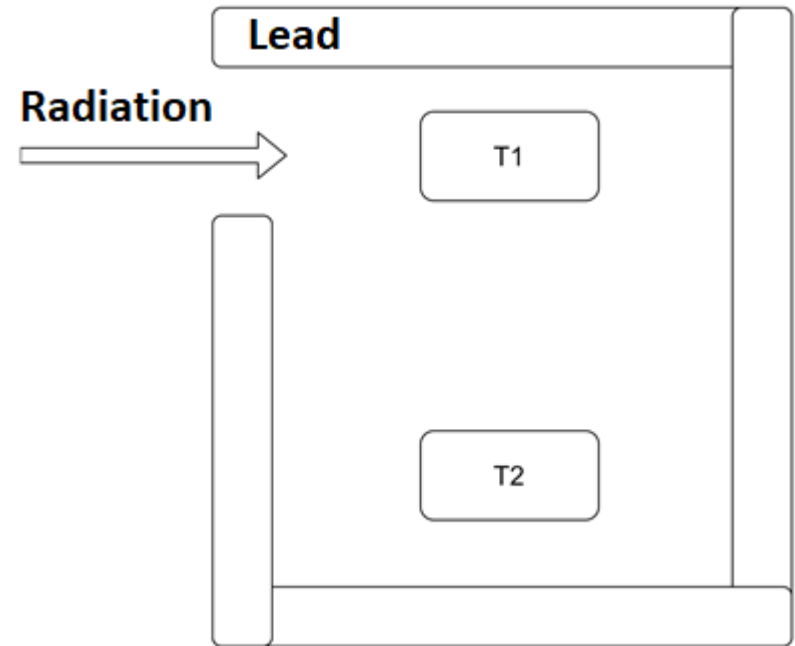
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- Calorimeters
- Gas-filled (ionization) detectors
- Semiconductor detectors
- Scintillation detectors
- Thermoluminescent detectors

Calorimeters

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- **For standard dose measurement**
- Used in “**primary**” laboratories for primary dose measurements
- **Secondary measuring instruments** can be calibrated against these
- Suitable **only for measuring high doses**
- Measurement is based on **thermal effect**
- Applicable to **any type of radiation**



$$D \sim T1 - T2$$

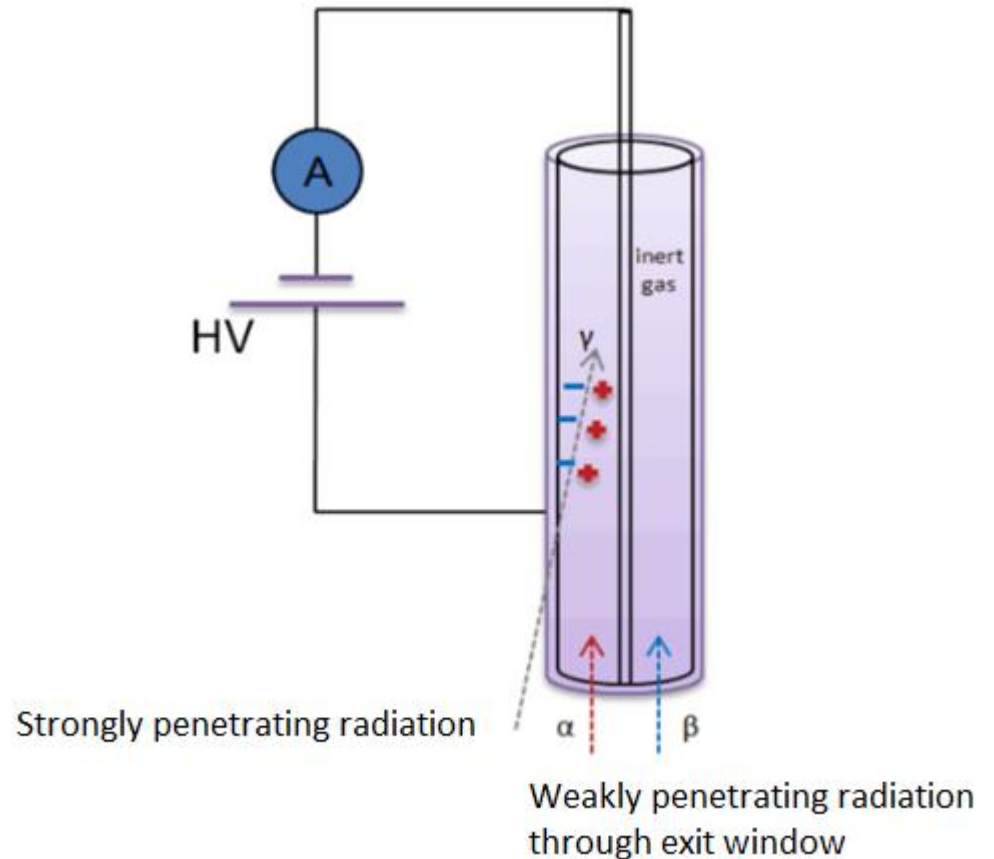
Gas-filled detectors

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- Gas-filled volume ($\sim\text{cm}^3$)

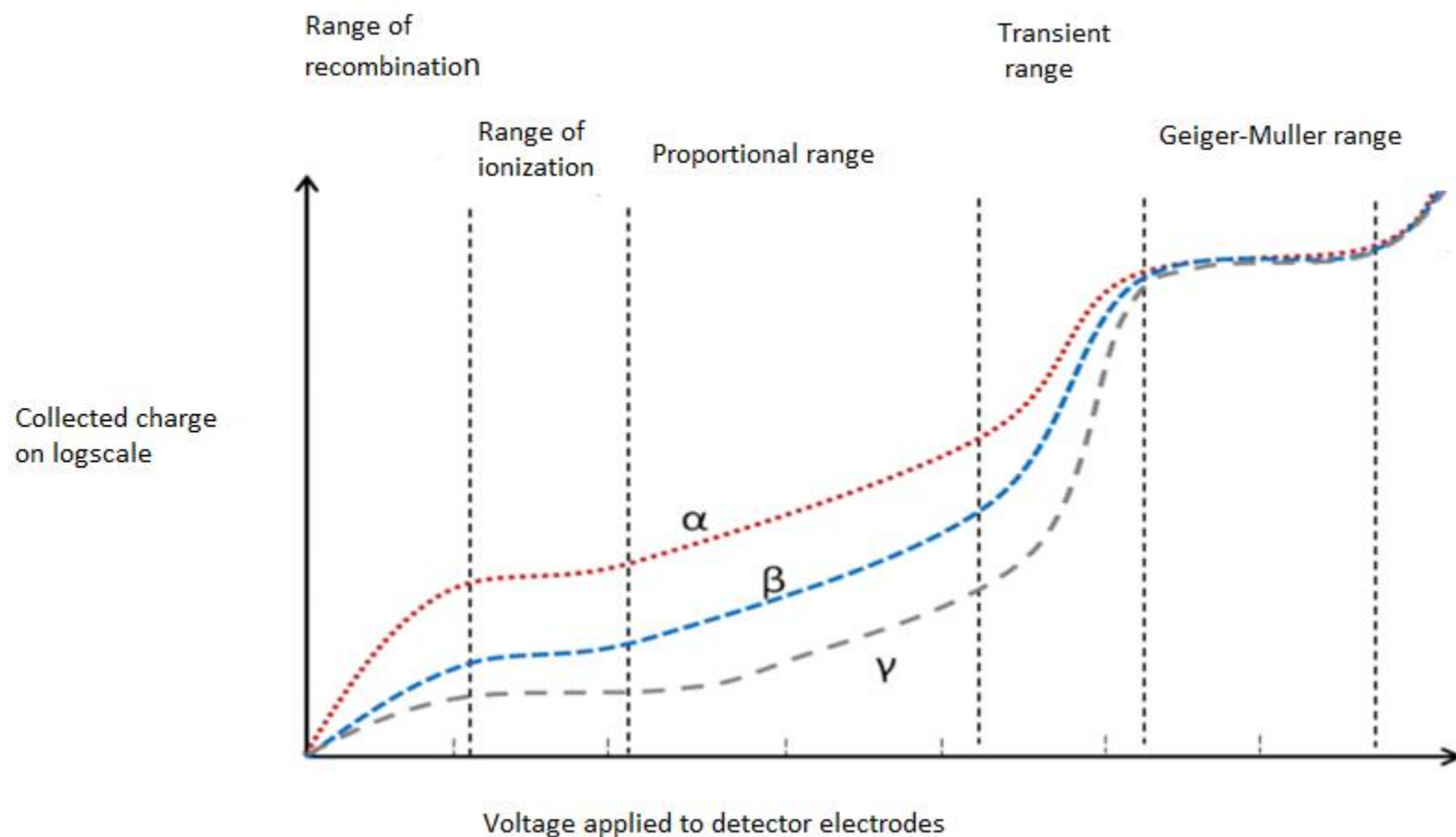


- Voltage applied to electrodes ($\sim 100\text{ V}$)
- Electronics for measuring collected charge ($\sim\text{pA}$)
 - Electrometer



Gas-filled detector measurement ranges

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Range of ionization chamber mode

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- Due to the voltage applied to the electrodes, the anode is able to collect the charges produced during ionization before they recombine.
- The measured charge is proportional to the number of ion pairs produced, which depends on the dose absorbed in the volume over the given time.
- The instantaneous current is therefore a function of the dose rate.
- Suitable for measuring **higher (therapeutic) doses/dose rates**.

Ionization chambers

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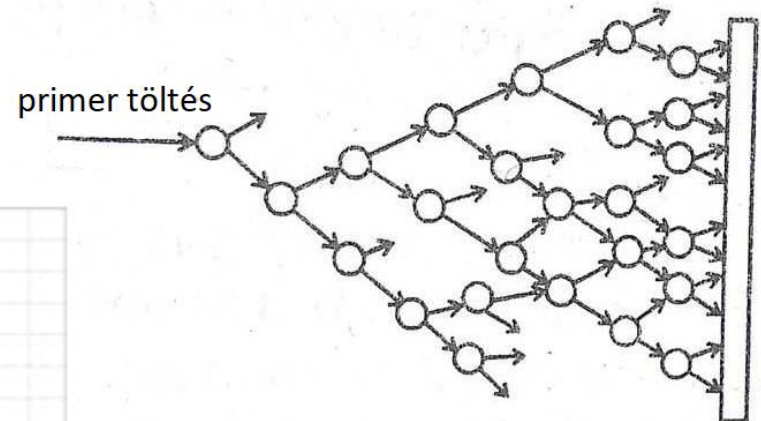
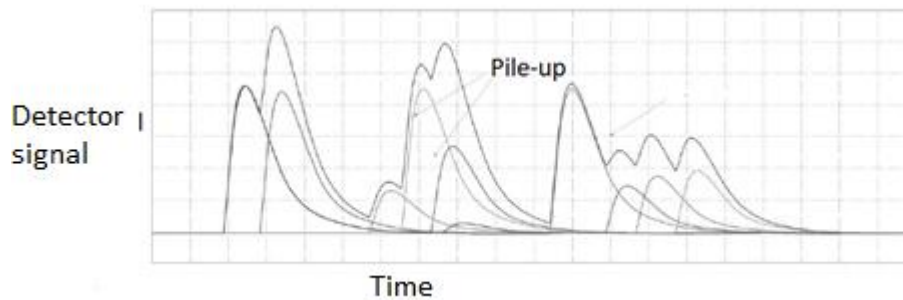
	Victoreen 451P	PTW 31013 (+ Unidos)
Sensitive volume	230 cm ³	0.3 cm ³
Temperature Range	-20°C .. +50°C	10° - 40°C
Humidity range	0 to 100%	10 - 80 %
Energy range (γ)	>25 keV	40 keV - 50 MeV
Maximal dose rate	50 mSv/h	28 Gy/s
Application	Radiation protection	Radiation therapy



Proportional counter

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- **Gas amplification occurs**
- The current pulse is proportional to the number of primary ion pairs, which depends on the radiation energy.
- With a **discriminator** and **multi-channel analyzer**, it can also be used for measuring spectral data.
- **Pile-up** may occur in higher intensity fields.



FH 40 G-L10 proportional counter

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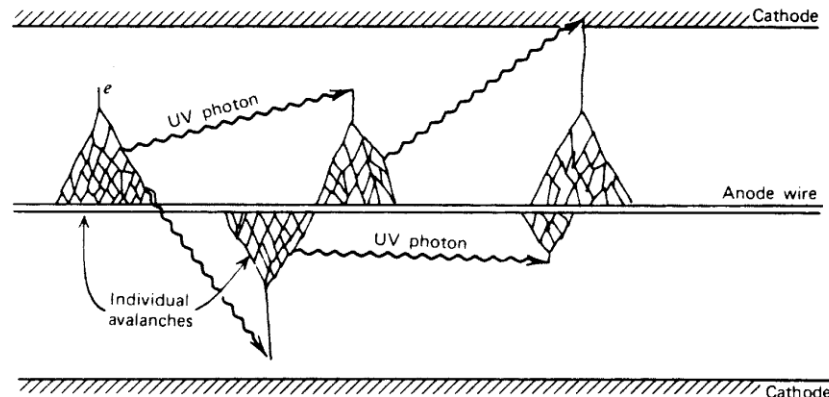
- **Energy-filtered proportional detector**
- **Energy range for photons:** 30 keV – 4.4 MeV
- **Measured quantity:** Ambient dose equivalent $H^*(10)$
- **Measurement range:**
 - Dose rate: 10 nSv/h -100 mSv/h
 - Dose: 0,1 μ Sv – 1 mSv



GM tube

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- Each individual particle produces a separate discharge, appearing as a uniform current pulse.
- **Self-sustaining gas amplification** occurs.
- Quenching is required in the detector volume.
- Due to the discharge processes, **dead time** occurs.
- Mostly suitable for measuring **lower dose rates**.



GM tube discharge

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- **External quenching:** via electronic means
- **Internal quenching:** using a quench gas, capable of absorbing the resulting ultraviolet radiation through internal conversion
- Organic gases (methane, alcohol)
- **Finite lifetime**
- **Halogen quench gas** is capable of recombination



Scintillator detector

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- Detection based on light phenomena
- The measured light intensity is proportional to the energy deposited by the detected particle.
- Photocathode: photon $\rightarrow$ electron
- Photomultiplier: signal amplification $\sim 10^3$

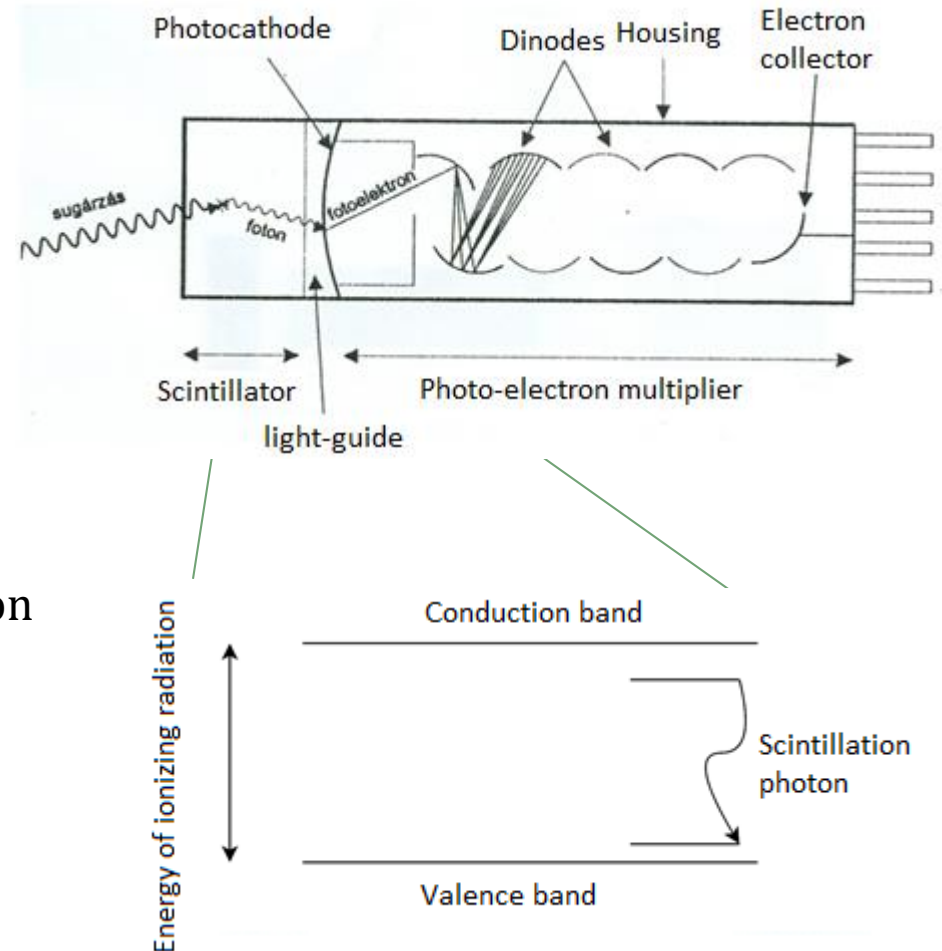
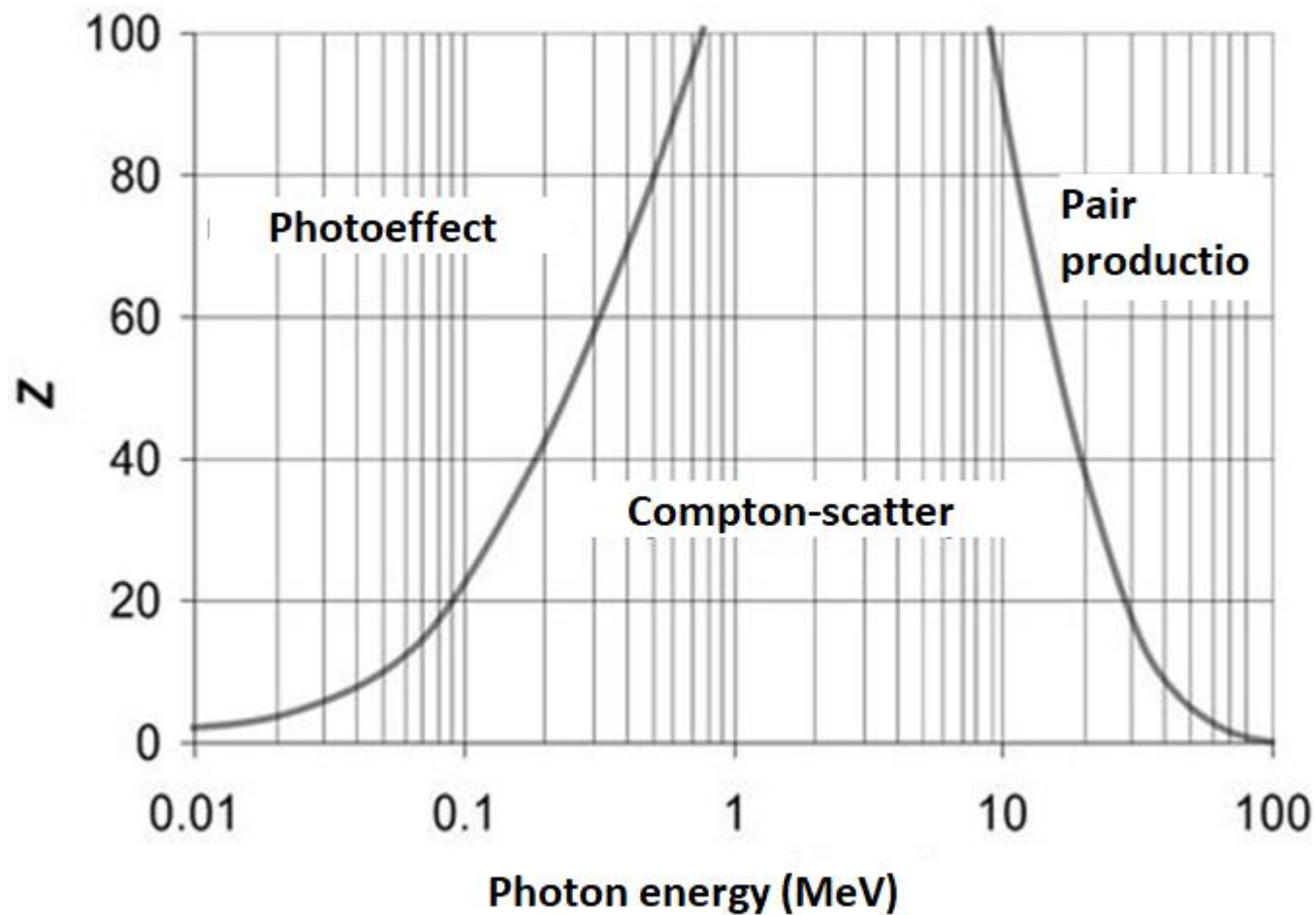


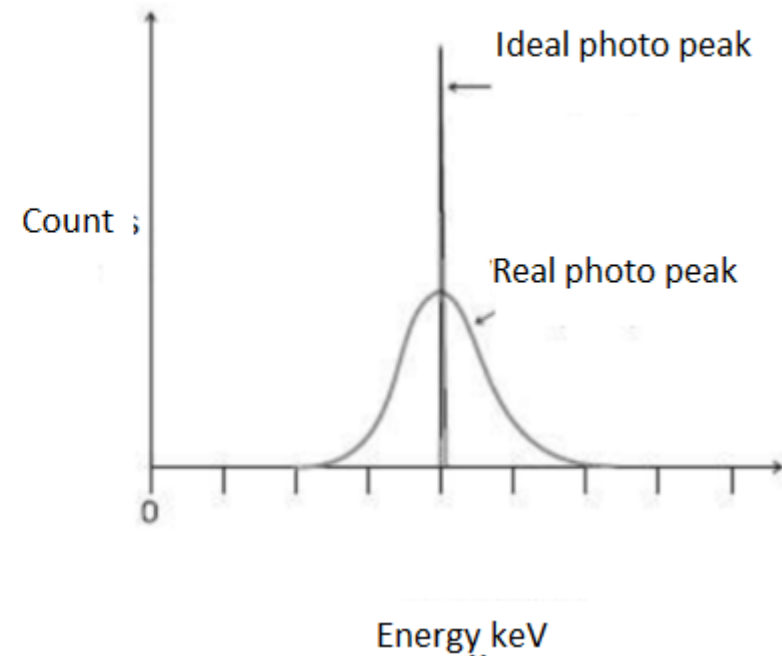
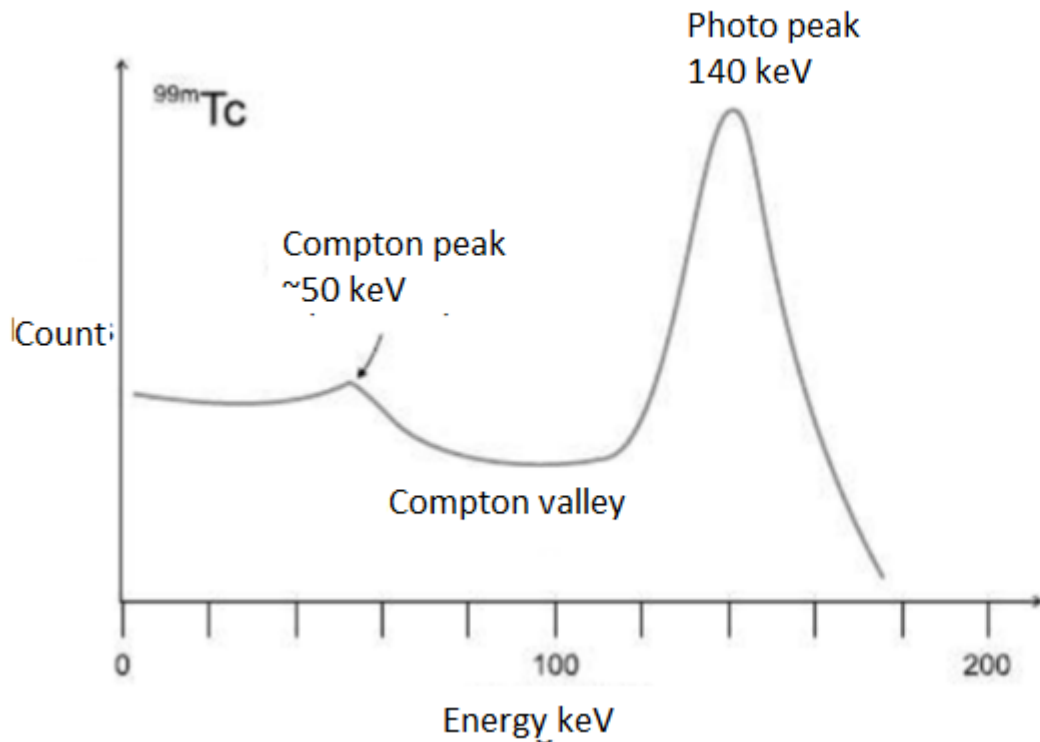
Diagram of interactions

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Spectrum of scintillator detectors

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Broadening in spectrum

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- Radiation → photon conversion efficiency
- Photon collection efficiency
- Photon → photoelectron conversion efficiency
- Photomultiplier: $\times 10^3$ amplification, statistical noise

At the same time:

- Even a single particle can be detected
- Wide measurement range in energy

Common scintillator crystals

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Scintillator material	Density g/cm ³	Effective Z	Probability of photoeffect (%)	Photon yield (photon/MeV)
BGO	7,1	75	40	9 000
LSO	7,4	66	32	30 000
NaI:Tl	3,67	51	17	41 000
LYSO	7,1	75	32	32 000
YAP	5,5	33,5	4,2	17 000



Scintillator detector

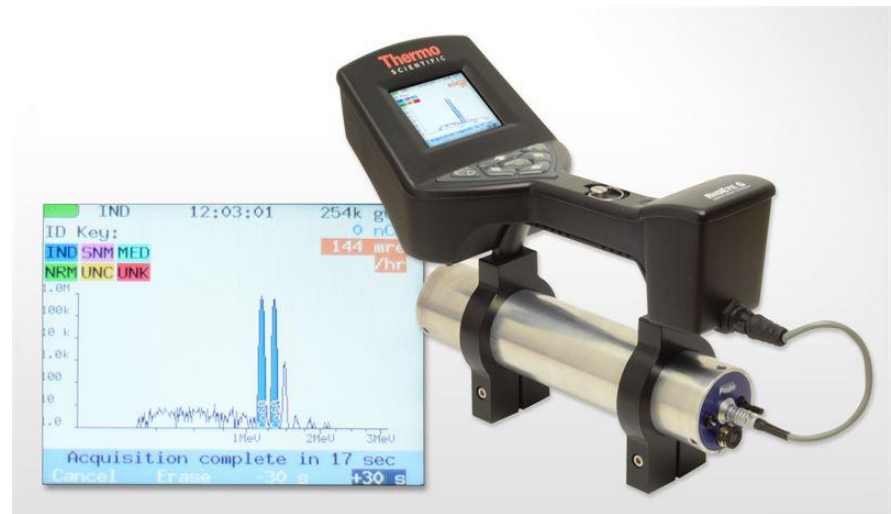
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- Radiation type: Gamma
- Energy range: 20 keV – 3 MeV
- Temperature range: -20° to 50°C
- Nuclide library: ANSI
- Detector dimensions:

2 inch x 2 inch NaI

1.5 inch x 1.5 inch LaBr

3 inch x 3 inch NaI

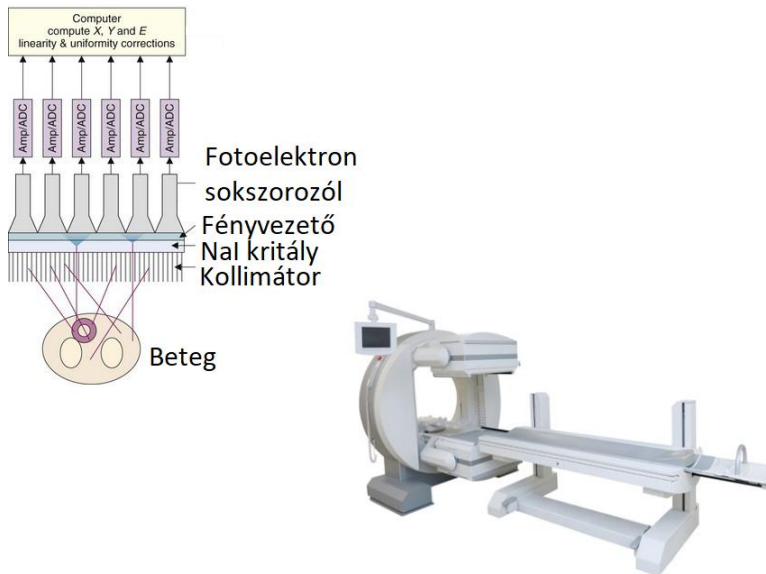


Application of scintillator detectors

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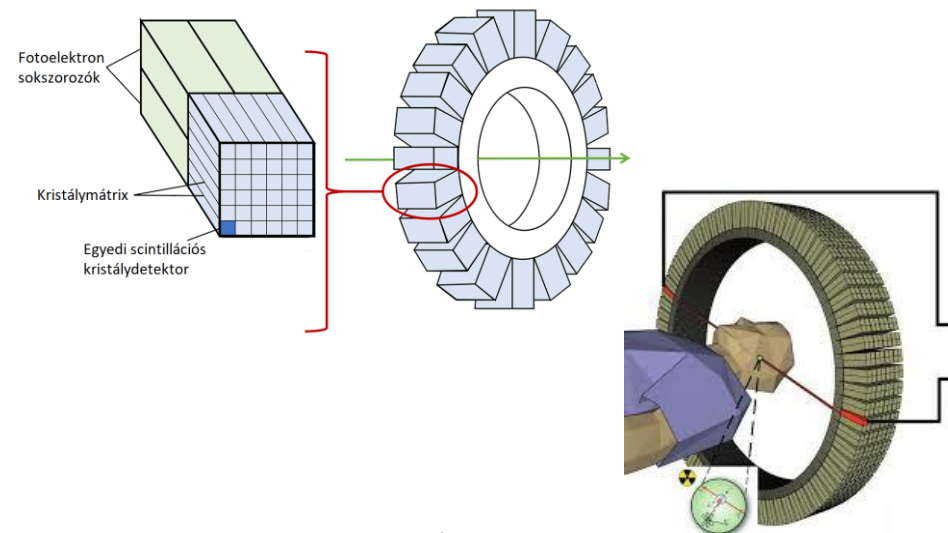
Gamma camera

Single crystal + position-sensitive photomultiplier



PET detector

Crystal matrices + photomultiplier per unit

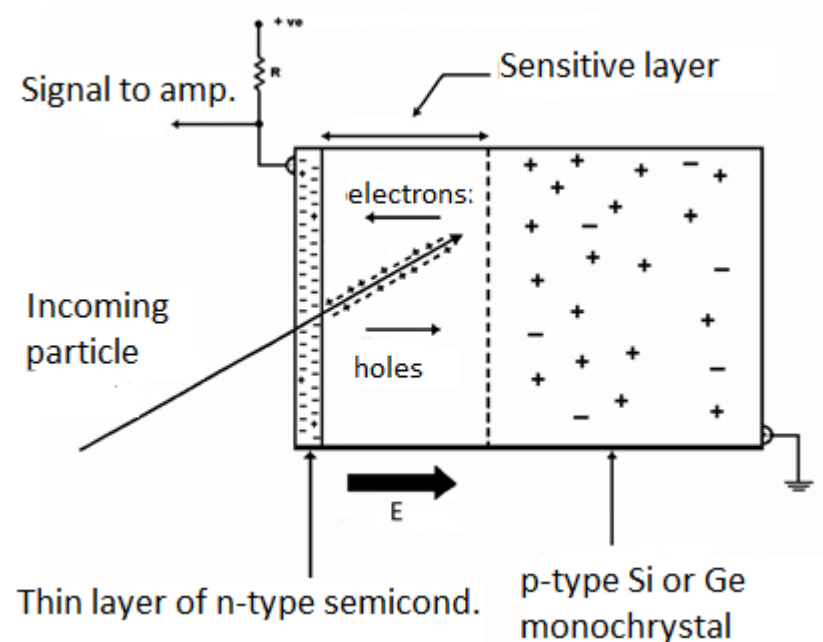


Semiconductor detectors

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In a reverse-biased diode, electron-hole pairs are generated in the depleted layer and are collected.

- Energy-selective detection → spectral information
- High density, good detection efficiency
- Small energy gap in the forbidden band



Si and Ge semiconductor detectors

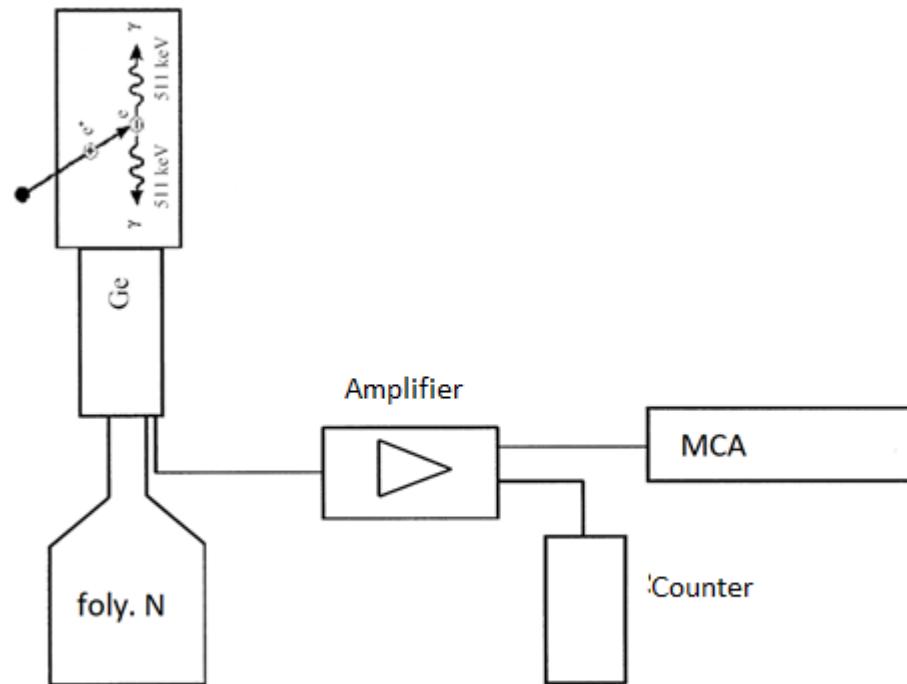
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	Ge	Si
Z	32	14
Relative atomic number	72,6	28,1
Density at room temp. [g/cm ⁻³]	5,33	2,33
Energy of e-hole production [eV]		
At room temperature	-	3,76
At 77 K	2,96	3,62

For NaI crystals, this value is around 40 eV, meaning that **10 times more primary charges** are generated in semiconductor detectors when detecting a particle of the same energy.

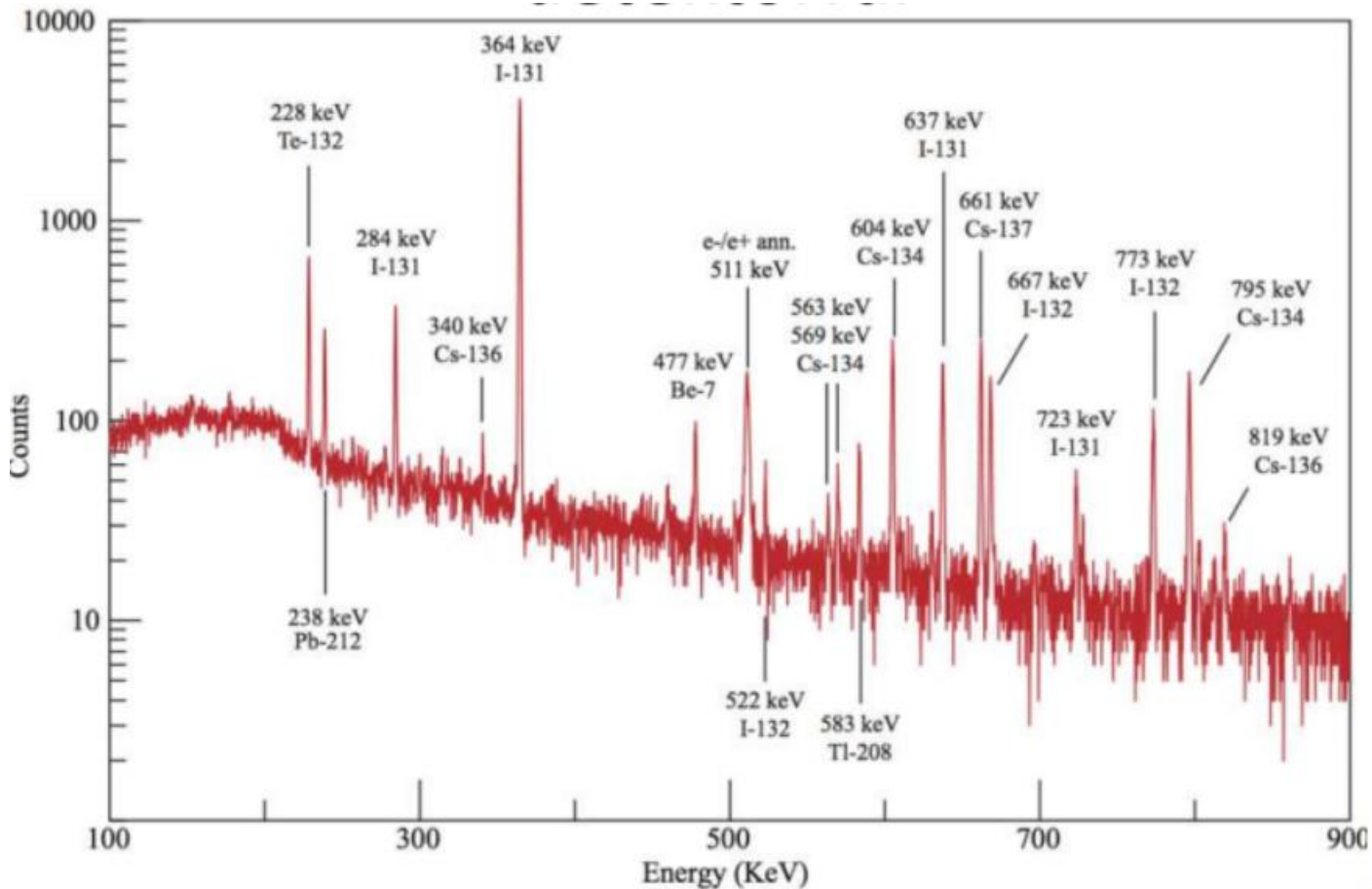
HPGe detector

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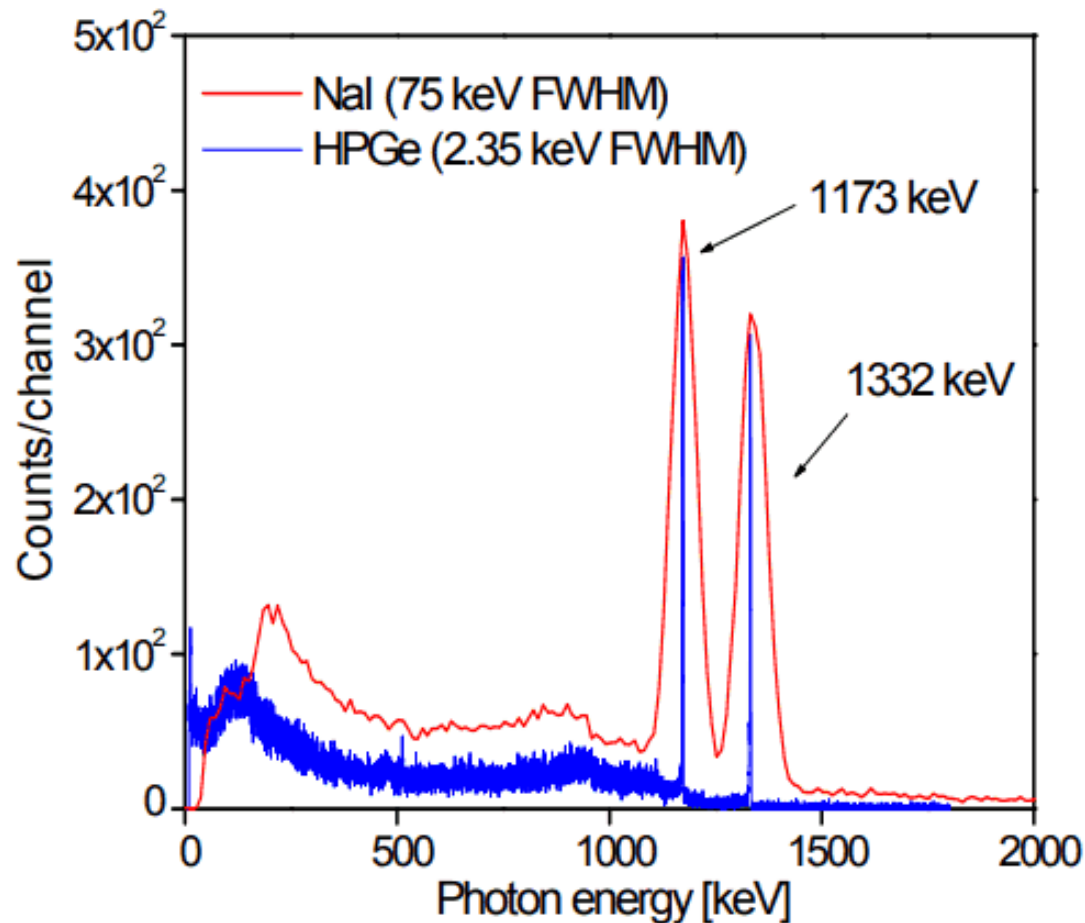
Spectrum of semiconductor detector

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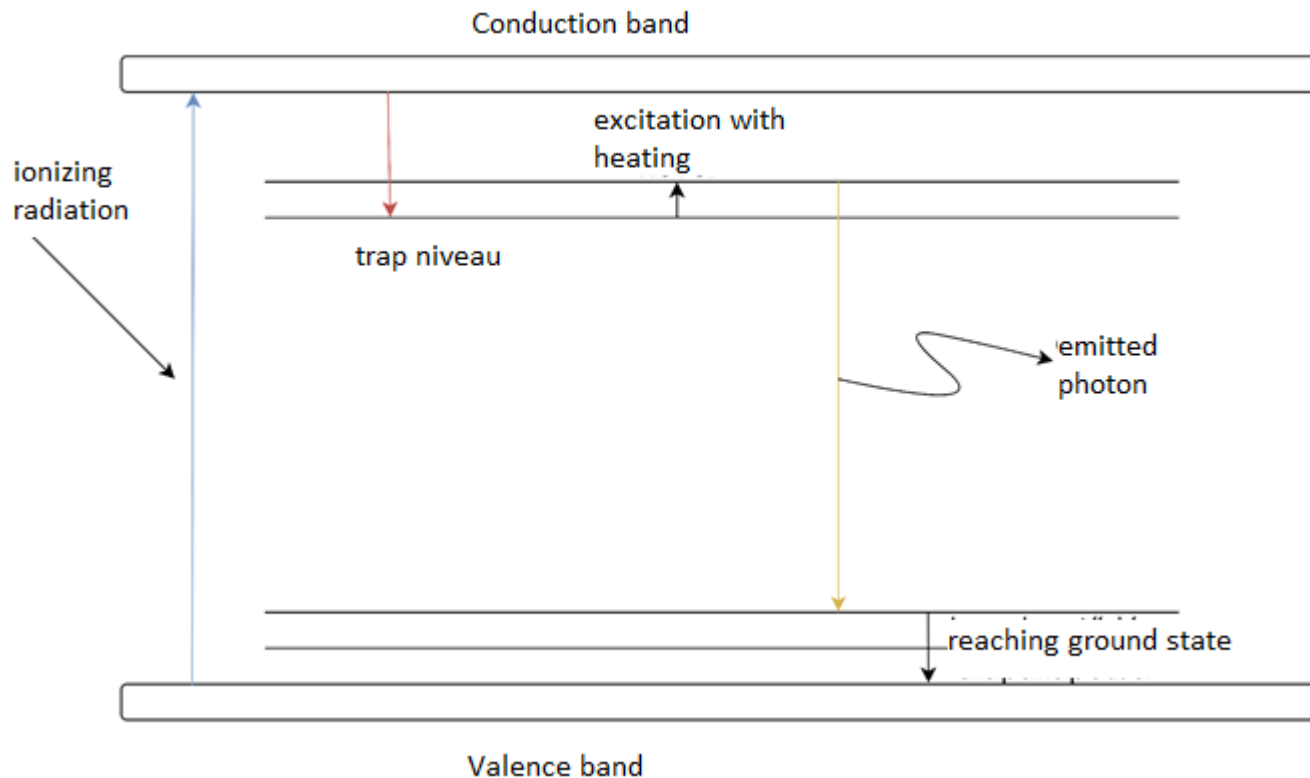
Boadening for NaI and HPGe detectors

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Thermoluminescent dosimeters

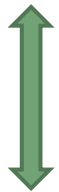
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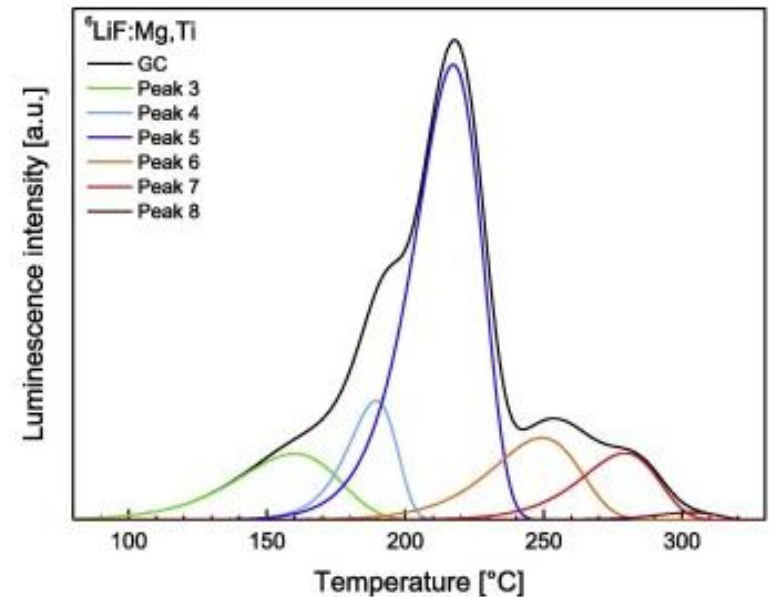
Thermoluminescent dosimeters

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- Small size
- Low cost
- Reusable
- In vivo dosimetry



- Measurement data is erased, one chance to read out
- Post hoc results
- Time-consuming
- Calibration and preparation required



Glow curve

TLD in personal dosimetry

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- **Passive detectors**
- **Cumulative dose**
- Dose accumulation over **2 months**
- Evaluated by the **National Personal Dosimetry Service**
- Can be retrieved from the **National Personal Dosimetry Registry**



Personal dosimeter- UD802AT

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Dosimeter	UD802AT
# of TL detectors with filters	4 db
Gamma energy	10 keV ... 10 MeV
Dose range	10 μ Sv ... 10 Sv
Detection limit	1,6 μ Sv
Cycles of readouts	> 1000
Fading	5% / év

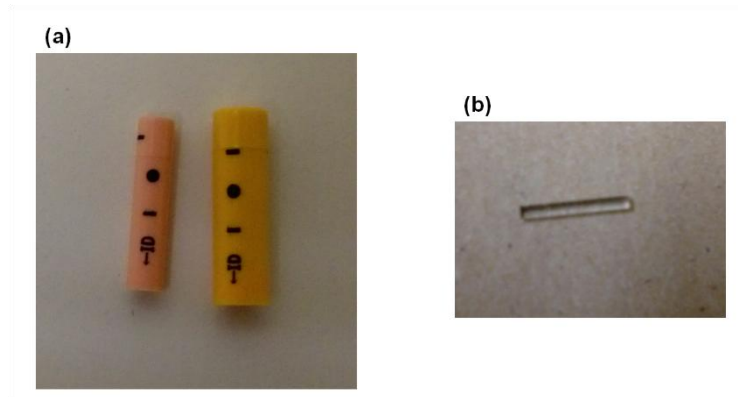
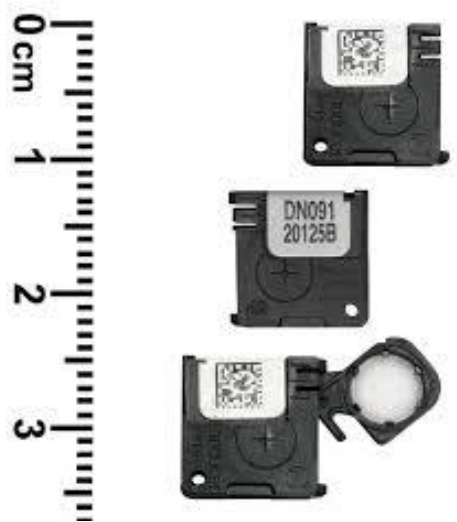
TLD alternatives

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OSLD – Optically Stimulated Luminescence Dosimetry

RPLD – RadioPhoto Luminescence Dosimetry

- Luminescence stimulated by light – instead of heating
- Measurement results can be read multiple times



Alternatives for personal dosimetry

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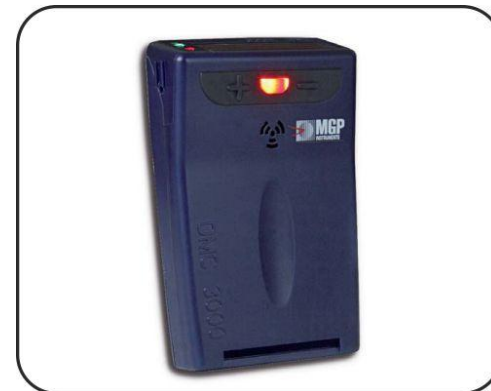


Film dosimeters

- Cumulative dose
- Selectivity achievable with filters
- Can be read multiple times in the short term
- However, cumbersome storage and evaluation procedure

Electronic dosimeters

- Cumulative dose, suitable even for monitoring very short operations
- Possibility to store data
- Application of warning levels
- Electronic auxiliary functions (reset, close-range data transfer, etc.)



Surface contamination measurement

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Contamination detection

- End-window GM tube
- Some proportional counters
- Low-activity gamma

contamination is poorly
measurable

Qualitative analysis of contamination

- With a proportional counter
- With a scintillation detector



RadEye AB100

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- Dual-phosphor scintillator
 - ZnS scintillator for alpha particle detection
 - Plastic scintillator for beta particles
- Field measurement auxiliary options:
- Headphones for noisy environments
 - >1000 hours battery life
 - Audio signal for alpha and beta particles, with increasing frequency proportional to the count rate



RadEye B20

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Similar mobile measurement support functions

Extension rod for higher activity

Use of filters for selectivity

Application	Contamination $\alpha\beta\gamma$	Contamination $\beta\gamma$	Dose Rate $H^*(10)$	Dose Rate $H'07$
Autodetection Filter	No Filter	Alpha Blocker 425068581	H*(10)Filter 425068582	H'07 Filter 425068583
RadEye B20 / B20-ER				
Filter Code displayed at the LCD	No Code	(α Blocker)	(H*(10))	(H'07)
Related Units	cps cpm Bq/cm ² Bq dpm dps	cps cpm Bq/cm ² Bq dpm dps	Sv/h rem/h	Sv/h rem/h



Neutron detection

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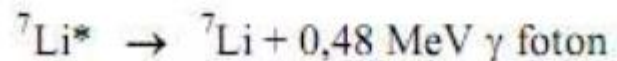
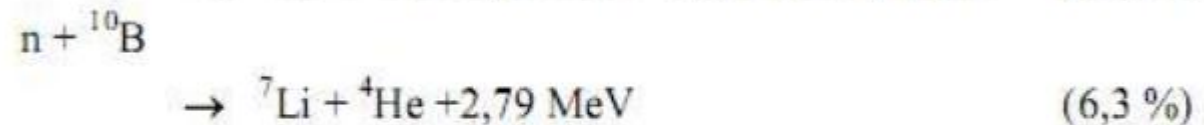
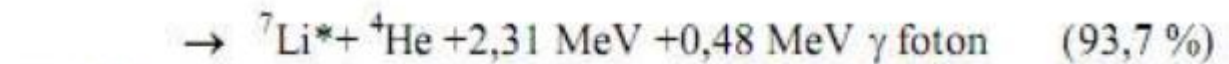
- **Difficult to detect** due to the low interaction probability, especially for fast neutrons.

Neutron thermalization is required for measurement.

A **gas-filled proportional counter** surrounded by a **moderator medium** is used.

The fill gas is mostly **BF₃**.

The neutron interacts with **boron**, and the resulting photon can be detected



Neutron detectors ($H^*(10)$)

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	Wedholm 2222A	Berthold LB 6411	Thermo Scientific FHT 762
Detector	BF3	3He/CH4	3He
Moderator	PE(B)	polietilen (2% carbon)	polietilen/ tungsten
Energy Range	0,025 eV- 17 MeV	0,025 eV- 20 MeV	0,025 eV – 20 MeV
Dose rate range	1 μ Sv/h- 1000 mSv/h	30 nSv/h- 100 mSv/h	1 nSv/h- 100 mSv/h
Dead time	1 μ s	5 μ s	
Sensitivity	0,35...0,5 cps/ μ Sv/h	1,27 cps/ μ Sv/h	0,84 cps/ μ Sv/h
Average background count	0,0083 cps	<0,02 cps	
Gamma sensitivity	2 Gy/h <10 μ Sv/h@10 mSv/h	<40 μ Sv/h@ 10 mSv/h	1...5 μ Sv/h@ 100 mSv/h
Directional dependence	significant	-30%...+30%	-20%...+20%

THANK YOU!